

# A queueing-theoretical delay analysis for intra-body nervous nanonetwork



Naveed A. Abbasi\*, Ozgur B. Akan

Next-generation and Wireless Communications Laboratory, Department of Electrical and Electronics Engineering Koc University, 34450, Istanbul, Turkey

## ARTICLE INFO

### Article history:

Received 22 December 2014

Received in revised form 19 June 2015

Accepted 4 August 2015

Available online 12 August 2015

### Keywords:

Nanoscale communication

Neuro-spike communication

Intra-body nervous nanonetworks

Queueing theory

## ABSTRACT

Nanonetworks is an emerging field of study where nanomachines communicate to work beyond their individual limited processing capabilities and perform complicated tasks. The human body is an example of a very large nanoscale communication network, where individual constituents communicate by means of molecular nanonetworks. Amongst the various intra-body networks, the nervous system forms the largest and the most complex network. In this paper, we introduce a queueing theory based delay analysis model for neuro-spike communication between two neurons. Using standard queueing model blocks such as servers, queues and fork-join networks, impulse reception and processing through the nervous system is modeled as arrival and service processes in queues. Simulations show that the response time characteristics of the model are comparable to those of the biological neurons.

© 2015 Elsevier Ltd. All rights reserved.

## 1. Introduction

Applications of nanotechnology are being realized from nano-switches and actuators [1], to intelligent drug delivery [2], nanoscale sensing [3] and bio-hybrid systems [4]. Although the promise of nanotechnology is huge, the associated challenges are not small by any means either. Nanomachines face very small dimensions, scarce processing, limited memory resources and simple networking capabilities.

The human body is a huge nanoscale communication network, where individual entities such as organs or cells communicate by means of nanomachines to make an intelligent system on a macro scale [5]. Understanding the dynamics of molecular communication not only helps us advance our work in development of nanomachines, but also gives a new perspective to the science of disease and

treatment. Many diseases of the human body can in fact be quantified as various forms of communication system failures [6].

The nervous system forms one of the most complex communications systems. It is also one of the most studied systems because of its elegance and importance in the human body. Nervous diseases such as Alzheimer's disease, Schizophrenia and Parkinson's disease are key challenges for the world in terms of human disease in the current age.

Although the applications and information in a particular communication network may differ significantly, the methods for communication remain similar. Several studies on molecular communication [5–9] target the nervous nanonetwork to develop communication-theoretical understanding of the nervous system. These studies result in the formulation of various models of synaptic channels under different scenarios. On the other hand, [10–12] introduce models for biological systems based on layered queueing networks.

The advantage of using queueing analysis for biological networks lies in the fact that big networks such as central nervous system and the neural cortex can be viewed

\* Corresponding author.

E-mail addresses: [nabbasi13@ku.edu.tr](mailto:nabbasi13@ku.edu.tr) (N.A. Abbasi), [akan@ku.edu.tr](mailto:akan@ku.edu.tr) (O.B. Akan).

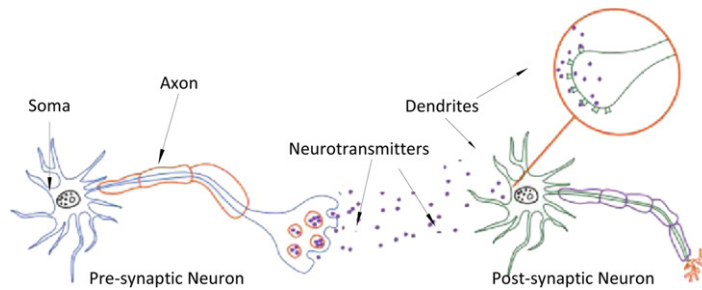


Fig. 1. Communication between a presynaptic and a postsynaptic neuron.

on the whole as a single network, thus making us able to study the collective behavior of these networks. To date, no work exists on the modeling of nervous nanonetwork from the queueing theoretical perspective. The motivation for such a model lies in a variety of applications from drug delivery to nervous disorder diagnosis. For example, in case of drug delivery, the nervous system can be viewed as the wired network of the body and target-specific drug delivery can be triggered by means of nerve impulses and neurotransmitters. Parameters such as the time required for a particular drug delivery and optimal rates of impulses to produce these scenarios can be viewed as queueing parameters. Additionally, the diagnostics of nervous disorders, where reflex latencies help in diagnosis, can benefit from such a model. Practitioners can move from using basic reflexes such as patellar reflex to more complex responses to improve disease diagnostics.

The objective of this paper is to derive a model of nanoscale neuro-spike communications between one input and one output neuron by using the fundamentals of queueing theory. We first develop an understanding of the neuro-spike communication and identify key blocks of the system. We then model these blocks using queueing theory implements such as queues and servers. Finally, we perform an analysis of response time characteristics of the model.

The remainder of this paper is organized as follows. We provide a brief overview of neuro-spike communication in Section 2. Section 3 presents the impulse transmission through the axon while Section 4 discusses the neurotransmitter propagation and reception in the synapse. Based on these analyses, we develop a queueing model of the neuron in Section 5. Results are presented in Section 6 and concluding remarks are provided in Section 7.

## 2. Overview

The fundamental task of a neuron is to receive, conduct and transmit spikes or impulses which are generated in response to external or internal stimuli. These impulses travel between various body parts and the central nervous system (CNS).

A single neuron can be divided into three main parts which are the dendrites, the soma or cell body and the axon. The communication between two neurons starts when an impulse traveling in a presynaptic neuron, also known as the action potential (AP), reaches the axon terminal. Fig. 1 shows two neurons in such a scenario. In order

for the AP to traverse from one neuron to the next, it needs to travel across the cell gap known as the synaptic cleft. Synaptic communication can be done either electrically or chemically.

In electrical synaptic communication, APs are transferred directly between two neurons by means of direct physical connections between them. On the other hand, in chemical synaptic communication, chemicals known as neurotransmitters are released in the synaptic space, also known as synaptic cleft, to achieve communication. Since chemical synapses occur more frequently, we focus our study on these.

Communication begins when the AP reaches the axonal terminals of the presynaptic neuron. The electrical depolarization of the cell membrane at the synapse causes Calcium ion ( $\text{Ca}^{2+}$ ) channels to open.  $\text{Ca}^{2+}$  ions then flow through the presynaptic membrane, rapidly increasing the calcium concentration in the interior of the cell membrane. This in turn activates a set of calcium-sensitive proteins attached to membranous sacks called vesicles that contain neurotransmitters to fuse with the membrane of the presynaptic cell. The fused membranes start to dump neurotransmitters into the synaptic cleft. The neurotransmitters drift across the synaptic cleft and bind to receptors present on the dendrites and the cell body of the postsynaptic neuron. The receptors are ligand-gated ion channels which open upon binding with a neurotransmitter. These channels create paths for ions to enter and leave the cell membrane of the postsynaptic neuron. Ions which are higher in concentration outside the cell membrane, flow inside the cell body causing a local depolarization. Each of these local polarization causing channels creates a potential change known as Excitatory Post Synaptic Potential (EPSP). The overall depolarization is a sum of all the EPSP and is proportional to the size of the stimulus, strength of the synapse or the amount of neurotransmitters released.

The depolarization causes the membrane threshold to rise from a base value of  $-70$  mV to about  $-50$  mV. At this stage, the depolarization is not powerful enough to traverse through the entire neuron so it needs to be amplified along its way. When the depolarization reaches the Axon Hillock, voltage-gated Sodium ( $\text{Na}^+$ ) and Potassium ( $\text{K}^+$ ) ion channels open. These form a positive feedback causing neighboring voltage-gated channels further along the axonal body to open. The depolarization thus travels further along the axon. The  $\text{Na}^+$  channels become inactivated when the depolarization peaks at around  $70$  mV. The  $\text{K}^+$  channels then normalize the cell polarization afterwards.

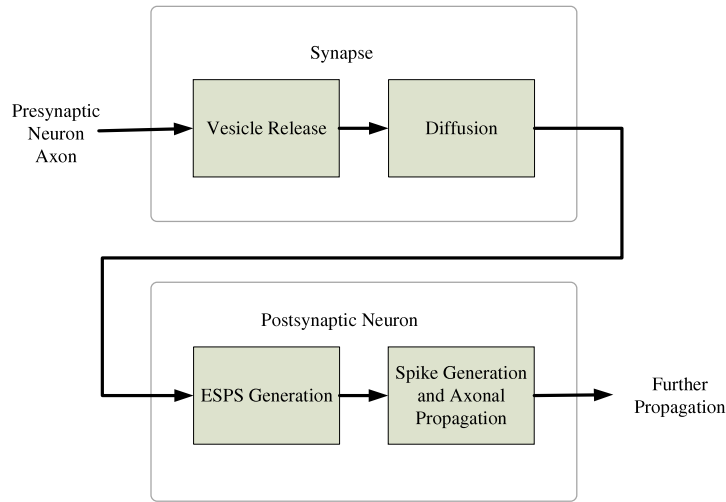


Fig. 2. Functional block diagram of neuro-spike communication.

The AP travels through the axonal body until it reaches the axonal terminal repeating the same operations with further neurons.

Fig. 2 shows a functional block diagram of neural communication. We see that the AP in a presynaptic neuron causes vesicle release in the synaptic cleft causing the diffusion of the neurotransmitter, EPSP generation at the postsynaptic neuron and spike propagation through the axon. All these processes can be loosely grouped under two types of transmissions namely, the synaptic transmission and the axonal transmission. Since our model is from a queueing perspective, we look at these processes in terms of the service times required by these processes as well as the distributions of arrivals in these transmission networks.

### 3. Axonal transmission

In this section, we develop an understanding of axonal communication and identify the arrival and processing of APs through the axon. This analysis helps identify the queueing model for an axon. To simplify additional analysis, we will further identify dendritic transmission and somatic summation of the EPSP signals in this section as well.

Axons act as the transmission lines of the nervous system with diameters on the order of a few micrometers and are either unmyelinated or myelinated. Myelinated axons are covered by a sheath of a fatty dielectric substance called myelin. Since the axons carry electrical signals, insulation due to myelination creates a positive effect on the conduction enabling a rapid and better electrical propagation. Once the impulses reach the end of the axon, they terminate in the axonal terminal causing neurotransmitter release from vesicles. Although, the process is very complex, a few studies have identified the real-time latency of this release operation [13].

#### 3.1. Arrival of impulses

Axonal transmission starts with the arrival of impulses in the axon. Although the impulse sources for CNS are very

diverse, most of these can be modeled as Poisson processes. In fact, several impulse sources for human nervous system are already known to be Poisson processes. These include the arrival rate of photons in human eyes, as well as sensations through the olfaction or gustation [7, 14]. Therefore, the arrival of impulses in an axon can be modeled as a Poisson process.

#### 3.2. Axon as a cable

The best way to analyze the operation of an axon is to consider the operation of an axon as that of a transmission cable. Cable theory [15] provides us with such an axon model. Assuming that passive conduction occurs as the impulse is conducted through an axon, axons are modeled as cylinders composed of infinitesimal segments as shown in Fig. 3. Here,  $c_m$  is the capacitance due to electrostatic forces across the axon membrane,  $r_m$  is the membrane resistance per unit length,  $i_m$  is the membrane current,  $r_i$  is the axoplasmic resistance per unit length within the axon,  $i_i$  is the axoplasmic current,  $r_o$  is the resistance per unit length outside the membrane and  $a$  is the radius of the axon.

The cable equation for the above model by [15] is

$$\lambda^2 \frac{\partial^2 V(x, t)}{\partial x^2} = V(x, t) + \tau \frac{\partial V(x, t)}{\partial t} \quad (1)$$

where  $V(x, t)$  is the function for potential difference with respect to distance and time,  $\lambda$  is the length constant defined as  $\lambda = \sqrt{r_m/r_i}$ , and time constant  $\tau$  is given as,  $\tau = r_m c_m$ .

The length constant indicates how far a charge can flow along a cable. Since  $\lambda$  is proportional to the square root of membrane resistance per unit length,  $r_m$ , the greater the values of  $r_m$ , the farther a charge can travel inside an axon. Myelinated axons have higher membrane resistance than unmyelinated neurons so their length constants are higher as well. That is the reason why APs can travel more reliably for longer distance in much thinner myelinated neurons in comparison with unmyelinated neurons. Refs. [16, 17]

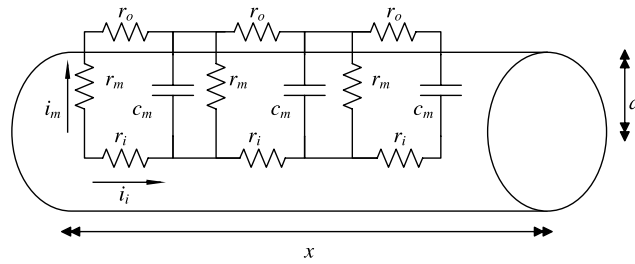


Fig. 3. Cable theory model of axon.

show that as the frequency of the input signal to a neuron increases, APs attenuate much faster because the length constant decrease that is occurring is proportional to increase in the internal resistance  $r_i$ . This shows that there is a frequency dependence of the axonal transmission as well.

The time constant  $\tau$  determines how fast the membrane potential responds to a current in the axoplasm. Thus, the larger the membrane capacitance,  $c_m$ , the longer it takes for a section of the membrane to get charged or discharged.

Suppose  $V_x$  is the voltage at a given distance  $x$  from one end of an axon, it is given as a solution for (1) by [15] as

$$V_x = V_0 e^{-x/\lambda} \quad (2)$$

where  $V_0$  is the potential at the point of impulse initiation. Based on (2), we analyze and compute the time a signal takes to travel through an axon and the level of signal attenuation at a certain distance.

### 3.3. Conduction speed of an axon

One of the parameters most commonly found by experimental studies for various axons is the conduction speed through an axon. Lengths for various neuron types are fairly easy to find experimentally. Thus, the time required for a transmission through that axon can be calculated based on the conduction speed through an axon.

Let us consider an AP traveling along an axon such that it faces no attenuation. The conduction speed,  $s$ , is given as the derivative to distance traveled with respect to time.

$$s = \frac{dx}{dt} \quad (3)$$

If a voltage  $V(x, t)$  of the AP is also moving in  $x$  direction, [18] shows that

$$\frac{\partial^2 V(x, t)}{\partial t^2} = \frac{s^2}{d} 4 \cdot \rho \cdot I_m \quad (4)$$

where  $d$  is the diameter of the elements from Fig. 3,  $\rho = r_i \cdot \pi \cdot a^2$  is the resistivity of the axoplasm and  $I_m$  is membrane current density given by  $I_m = i_m / (\pi \cdot d)$ . Eq. (4) can also be re-written as

$$s = \sqrt{\frac{\partial^2 V(x, t)}{\partial t^2} \frac{d}{4 \cdot \rho \cdot I_m}} \quad (5)$$

Thus, the conduction speed of an axon is directly proportional to the square-root of its diameter. This characteristic of the axonal communication is observed in most experiments based on axonal communication [19,17].

In [20], the authors perform this analysis further and identify the conduction speed of unmyelinated axons as

$$s_{nm} = \sqrt{\frac{d}{8 \cdot \rho \cdot c^2 \cdot r^*}} \quad (6)$$

where  $c$  is the membrane capacitance per unit area and  $r^*$  is the resistance per unit area.

### 3.4. Na<sup>+</sup> channel inactivation

Before an AP is transferred, the axonal membrane is at rest and Na<sup>+</sup> channels are in a deactivated state. In response to an AP, these channels open, allowing the ions to flow into the axon and cause the action potential to grow. At the peak of an AP, when sufficient Na<sup>+</sup> ions enter the membrane, no further conduction is possible until a mandatory refractory period of Na<sup>+</sup> ion channels passes. This absolute refractory period is followed by a relative refractory period where the K<sup>+</sup> ions terminate the action potential by re-polarizing the membrane. K<sup>+</sup> ions, that move out of the cell, bring the membrane potential closer to the equilibrium potential for potassium. This causes brief hyper-polarization of the membrane making the membrane potential transiently more negative than the normal resting potential. Until the potassium conductance returns to the resting value, a greater stimulus will be required to reach the initiation threshold for a second depolarization. The return to the equilibrium resting potential marks the end of the relative refractory period. Although, conduction is possible after the absolute refractory period passes, this happens only in certain circumstances.

Mentioning this phenomenon is important because for a given axon, this causes an additional delay before a new impulse can enter and propagate through the axon. In [17], the authors show that the during the inactivation after an AP, new impulses fail. They also show that the inactivation period increases at lower temperature, although, for the purpose of this work we are looking at neurons operating at a physiological temperature of 37 °C only. Hence, the inter-arrival time between two impulses should be larger than the inactivation period of the Na<sup>+</sup> ion channels for reliable communication.

### 3.5. Dendritic and somatic transmission

Although there are differences in the sizes, shapes and physical properties of dendrites and axons, they have a similar function of conducting impulse signals. That is why,

both are modeled in a similar way by cable theory [21]. Dendritic trees can be modeled as parallel trees of cables or they could be lumped together as equivalent cables.

Assuming the average dendritic length of  $E[L_D]$  and a dendritic diameter of  $d_D$ , the average propagation time through a dendrite can be a modified form of (6) as the dendrites, when considered as cables that are not coated by myelin [22], the average delay an EPSP faces through a dendrite and the soma is given as

$$R_{DS} = R_{ion} + \frac{E[L_D]}{\sqrt{\frac{d_D}{8 \cdot \rho \cdot c^2 \cdot r^*}}} + R_{Soma} \quad (7)$$

where  $R_{ion}$  is the average ion channel inactivation time for a dendrite branch and  $R_{Soma}$  is the time for the EPSP summation and propagation from dendrites to the axon hillock.

The various EPSP signals generated by the dendrites are summed up as they move from the soma to the axon hillock. Since the communication is very secure, we can assume that there is a certain degree of synchronization in the EPSP arrivals. We will explore this further in the next section.

#### 4. Synaptic transmission

In this section, we discuss synaptic transmission which starts with neurotransmitter release from the vesicles and diffusion across the synaptic cleft. Neurotransmitter release can be identified by the arrival process in a queueing network whereas the diffusion and EPSP generation constitute the processing of the synaptic queueing network.

##### 4.1. Neurotransmitter arrival

Synaptic transmission starts by the arrival of neurotransmitters in the synapse. Neuro-spikes from the axon cause vesicles to move towards the cell membrane of the axon terminal and fuse with it. The neurotransmitters housed in the vesicles are then released in the synaptic cleft. Thus, neurotransmitter release can be thought of as the process by which the neurotransmitters arrive in the synaptic medium.

Neurotransmitter release is a random process in that even with the presence of neuro-spikes, vesicles might not be released or vice versa. The probability of such a scenario is quite low [23], therefore, if we ignore such cases, the release process depends directly on the arrival process of spikes.

##### 4.2. Diffusion through synapse

The neurotransmitters released in the synaptic cleft reach the postsynaptic neuron by means of diffusion through the synaptic medium. The linear diffusion equation governs this process of diffusion [7] given as

$$\frac{\partial c(x, t)}{\partial t} = D \nabla^2 c(x, t) \quad (8)$$

where  $c$  denotes the concentration and  $D$  denotes the diffusion coefficient. Considering Gaussian diffusion, the

solution of the diffusion equation in an  $n$ -dimensional space from a position  $x$  is calculated by the theory of Green's function as

$$G(x, t) = (4\pi Dt)^{-n/2} \exp\left[\frac{-(x - x')^2}{4Dt}\right] \quad (9)$$

where Green's function tells us how a point of probability density initially at position  $x$  evolves over time and  $n$ -dimensional space. The PDF in (9) exists under the condition of normalization stated as

$$\int_{-\infty}^{\infty} G(x, t) dx = 1. \quad (10)$$

Assuming that diffusion for the current problem is a homogeneous process in one dimension, we modify (9) as

$$G(x, t) = \frac{1}{\sqrt{4\pi t}} \exp\left[\frac{-(x - x')^2}{4t}\right]. \quad (11)$$

Eq. (11) along with the condition provided in (10) describes the time distribution for diffusion of a neurotransmitter from one neuron to the next.

##### 4.3. EPSP generation

When neurotransmitters reach the ligand-gated channels present on the dendrites and soma of the postsynaptic neuron, they attach to these channels and a flow of ions starts between the cell and its surroundings. This causes EPSP to be generated at each of these channels. The EPSP generated at each of these ligand-gated channels is independent from EPSP generated from other channels. Subsequently, the cell body sums these independent EPSP to generate a potential difference. If this potential difference is above the threshold voltage, an AP is generated in the postsynaptic neuron, following a positive feedback amplification of the EPSP. Otherwise, the EPSP pulse dissipates without causing an AP in the postsynaptic neuron. The number of neurotransmitters that successfully attach to the ligand-gated channels depends on the number of channels available at a time and the concentration of the neurotransmitters in the synapse [24].

When neurotransmitters diffuse through the synaptic cleft to reach ligand-gated channels, not all the neurotransmitters are attached to these gates. The remaining neurotransmitters remain in the synaptic gap until they attach to one such gate, degrade or are re-uptaken by the axon terminal of the presynaptic neuron. A single action potential might give rise to several action potentials in the postsynaptic neuron if a significant amount of neurotransmitter has been released and the corresponding half-life is large enough to instigate another action potential [25]. Considering the neurotransmitters as information carrying packets in the synaptic system, we see that the degradation or re-uptake of the neurotransmitter in the synapse while it is not attached to the channel is analogous to a packet leaving the queue or a packet being dropped because of time to live (TTL) constraint.

In order to simplify the system, let us consider a single gate attachment as a service by the ligand-gated channel server and neurotransmitters that could not attach are



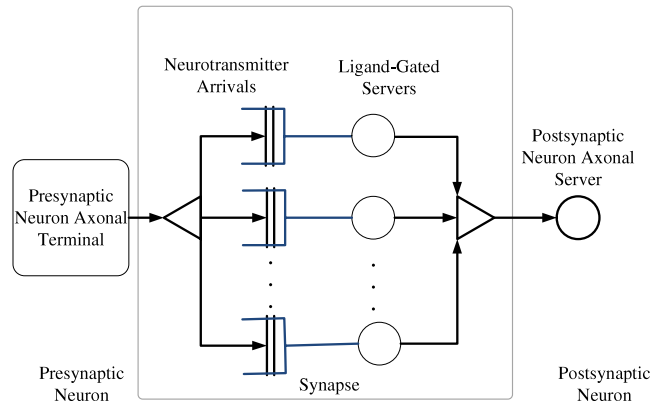


Fig. 4. Single-input single-output neuron queue model.

considered as waiting for the attachment chance. The analysis for the complex and random process of neurotransmitter attachment is very challenging otherwise because there might be cases where a single neurotransmitter might get attached to the channels several times and another neurotransmitter might not get attached at all [24]. Since all the neurotransmitters carry similar information, we can consider the attachments in a series one after the other. Thus, by wait we mean that a significant concentration of neurotransmitters will remain in the synaptic cleft. This assumption will be especially necessary in the case where a stimulation frequency is frequent. In such a case the synapse will have a concentration of the previous neurotransmitter release before a new impulse arrives [13].

## 5. Neuron queueing model

To view the neuron from a queueing perspective, we need to break down the neuron model into queueing constituents namely, the servers and the buffers/queue.

Fig. 4 illustrates a diagram of the proposed model. We assume that there are two major constituents of the system. The first constituent of the system is a fork-join queueing network that deals with neurotransmitter release, synaptic diffusion, dendritic propagation and EPSP generation. The number of branches of this fork-join synaptic queue is equal to the number of ligand-gated channels available for neurotransmitters attachment. To simplify the process, we assume that all the services of the synaptic communication are performed at the ligand-gated channels and each such receptor channel acts as a server. The synapse would thus act as the buffer of the system. The identification of the synapse with a queue is natural because when one neuron is trying to communicate with another, its respective neurotransmitters remain or buffer in the synapse while a previous impulse is being serviced by a neuron. In case that a single presynaptic neuron is in communication with multiple postsynaptic neurons, the synapse will still act as a queue. Each neuron will have its own fork join queue before its ligand-gated ion servers further serving their own axonal server. There is no condition on how the synaptic queue is shared between these servers as long as the number of available neurotransmitter is greater than the number of ligand-gated channels which is usually the case [13,24].

The second constituent is composed of just a single server. This server models the propagation of neuro-spikes through the postsynaptic neuron axon. The absence of a queue in the network relates to the fact that an axon can serve only one impulse at a time and does not contain any buffer where another incoming impulse can queue. It is, however, possible for a physical axon to have more than one impulse coursing through it at a time. This is because once the  $\text{Na}^+$  absolute refractory period is over, a new impulse may be generated in the axon by a new somatic EPSP summation. This is especially true for longer axons in bigger animals where refractory periods are a fraction of the total propagation time. The reason for still keeping a single server in the axonal communication is that if we look at the system from the perspective of an incoming impulse, it will still be served by the single axonal server after being served by the synaptic queue. Any impulse that comes during the refractory period would not be entertained. The discipline of this axonal server is first come first serve (FCFS).

The summation of the EPSP in the soma may or may not result in further spike generation. Thus, depending on a threshold it might end up in a sink or might be transmitted through the axonal body. The probability of failure  $p_f$  to go beyond the threshold voltage is usually quite low because neural communication is quite reliable as discussed in [19,17] but it is an essential parameter for any reliable model of communication [7]. In case there is a failure, further axonal propagation does not happen. Therefore, the second network is composed of single server queues with FCFS discipline queues in parallel.

### 5.1. Analysis of the synaptic transmission

#### 5.1.1. Arrival process

To make the analysis of the system simple, we have assumed that the dendritic propagation and the somatic communication are a part of synaptic communication. The assumption does not make any difference in our analysis other than providing a simplification by keeping the constituents of the fork-join network together.

The arrival distribution of the synaptic distribution depends on the departure distribution of the axonal server.

Several works on distributions of firing rate of neurons such as [26,27] identify the distribution of firing neurons to be Poisson. This is apparent from the analysis for axonal server given above as well. A Poisson input distribution to the axonal server, if deterministically served, generates an output which is also Poisson distributed.

### 5.1.2. Response time

The service time of the fork-join synaptic queue network involves several processes such as the time taken for neurotransmitter release for vesicles, time take for diffusion through the synapse and the dendritic propagation. In such scenarios, we often assume network service time distributions to be some unknown general distribution. Therefore under the analysis presented, we can say that the fork-join synaptic queue is a network of parallel M/G/1 queues.

The total response time of synaptic transmission  $R_S$  is a summation of the average vesicle release time  $R_{Ves}$ , average dendritic and somatic transmission time  $R_{DS}$  given by (7) and the average response time for diffusion through the synapse  $R_N$ .

$$R_S = R_{Ves} + R_N + R_{DS}. \quad (12)$$

It is difficult to model fork-join queues analytically and in fact, to date, analytical results exist for only two server systems [28]. Usually for more than two queues, approximations for mean response time exist in case of homogeneous servers. This suits the current analysis because the servers we are considering here are homogeneous in nature.

We assume that the parallel queues of neurotransmitters in the synapse are independent and identically distributed (i.i.d.). In [29], the authors have presented an approximation of the mean response time of a set of i.i.d. fork-join queues with M/G/1 queues in parallel service as

$$R_N \approx R_1 + \sigma_1 F_N \alpha_N \quad (13)$$

where  $R_1$  and  $\sigma_1$  are the mean response time and standard deviation, respectively, for one M/G/1 queue with no fork-join properties.  $F_N$  is a constant which scales according to the service time distribution of the servers and  $\alpha_N$  is a scaling factor that helps scale simulation results according to the results of a physical experiment.

If we consider a unit distance between the two neurons through the synapse, the PDF of neurotransmitter diffusion given in (11) can give us a service time distribution of neurotransmitter service for unit distance case. It should also be mentioned here that a normalization constant according to (10) should be multiplied so that the PDF does not exceed the unit area under the curve condition. Thus, the distribution of service time for a single M/G/1 neurotransmitter service is given as

$$G(t) = \frac{1}{\sqrt{4\pi t}} \exp\left[\frac{-1}{4t}\right] \exp\left[\frac{-t}{2.57 \cdot \pi}\right] \quad (14)$$

where the normalization constant  $\exp\left[\frac{-t}{2.57 \cdot \pi}\right]$  is approximated numerically to a precision of  $10^{-6}$ .

Since the failure rate of neurotransmitters generating an AP from their individual EPSP is quiet low in case of a valid stimulation to the presynaptic neuron [17], there must be a high degree of synchronization in their diffusion through the synapse. In other words, this means that the mean response times of each of the fork-join queues is quite similar. Thereby, the standard deviation term from (13) can be neglected for successful transmission case resulting in

$$R_N \approx R_1 = \int_0^{\infty} tG(t)dt. \quad (15)$$

## 5.2. Analysis of the axonal server

### 5.2.1. Arrival process

Any sum of EPSP above the threshold level of the presynaptic neuron generates an AP in the axon. The arrival of this EPSP excitation to the presynaptic neuron is a stochastic process. Since there can be several independent sources that produce the excitation, the arrival process at the axonal server can be considered as a Poisson process.

### 5.2.2. Response time

To determine the response time of an axon, we should first look at what constitutes the service of an axon. After an impulse enters an axon, as long as it is propagating within an axon, we consider it under service. Additionally, after an impulse leaves, the axon cannot have any further impulses pass through it until the  $\text{Na}^+$  ion channels return from their inactivation state. Thus, the total response time of an axon is a summation of the  $\text{Na}^+$  ion inactivation period and the response time for propagation through the axon body.

$$R_A = R_{Na} + R_{AP} \quad (16)$$

where  $R_A$  is the average response time of an axon,  $R_{Na}$  is the average time it takes for  $\text{Na}^+$  ion channels to become reactivated and  $R_{AP}$  is the average response time for impulse propagation through the axon.

Considering that the axons of a particular neuron type have an average length of  $E[L_A]$ , and conduction speed  $s$ , the average response time for propagation through such axons,  $R_{AP}$ , is given as

$$R_{AP} = \frac{E[L_A]}{s}. \quad (17)$$

Therefore, using (5), (6), (16) and (17), we can provide expressions for response time of an axon for any general case and for an unmyelinated neuron case as

$$R_A = R_{Na} + \frac{E[L_A]}{\sqrt{\frac{\partial^2 V(x,t)}{\partial t^2} \frac{d}{4 \cdot \rho \cdot l_m}}} \quad (18)$$

$$R_{A-nm} = R_{Na} + \frac{E[L_A]}{\sqrt{8 \cdot \rho \cdot c^2 \cdot r^*}} \quad (19)$$

We see that the response time of the axonal server depends on the conduction speed, diameter, length, resistivity of the axoplasm, the  $\text{Na}^+$  ion inactivation period and other physiological factors of an axon.

### 5.3. Total response time

Both the axonal server and the fork-join synaptic queue are in series, therefore, the overall mean response time of a neuron to a single impulse is the summation of the mean response times of the axonal transmission and the synaptic transmission.

$$R = R_S + R_A. \tag{20}$$

Eq. (20) can be written in its explicit form as

$$R = R_{Ves} + \int_0^\infty tG(t)dt + R_{DS} + R_{Na} + \frac{L}{\sqrt{\frac{d^2V(x,t)}{dt^2} \frac{d}{4 \cdot \rho \cdot l_m}}}. \tag{21}$$

This shows that the mean response time of a neuron depends on the diffusion characteristics, ion channel inactivation periods and the physical parameters of the neuronal structure. These characteristics match the results of previous neural communication models [6–8] and experimental results [19,14,16,17]. We see that the response time characteristics depend on propagation speed, axonal myelination and the diffusion distance through the synapse. Although our work is aimed at the Human nervous system, the results generated can be applied to any neuron type with provided characteristics.

An expression similar to (21) can be found specifically for unmyelinated neurons by using the value of  $R_{A-nm}$  instead of  $R_A$  in (19).

### 5.4. Impulses in the system

Apart from response time, other important measures of any queueing network are the number of customers in the system and its server utilization. These parameters become especially more useful when we are talking about a large network of queues. In our current scenario, customers in the system correspond to impulses present in a neuron.

We first consider the axonal server which is a single server system without any queue. Since there is no queue, at any given time, only one impulse can be served by the axon. Any other impulses that may come are rejected or dropped until the axon is ready to receive impulses again. The server utilization over a period of time, however, depends on the rate of impulse arrival at the axonal terminal. For any single server system, the arrival rate should be less than the service time for stable operation. If this rate is equal or beyond, the server utilization is hundred percent or in other words the neuron is maximally stimulated. The human body has several mechanisms in place to avoid such scenarios. However, tetanic contractions are one such example where a motor unit (muscle) is maximally stimulated by its associated neuron. This causes violent twitches in the muscles and can be lethal in certain cases. These contractions are usually the result of tetanus or the effect of toxic substances.

For the fork-join synaptic network, a queue exists in the synapse. To be stable, the arrival rate of the fork-join queue must be less than the sum of service rates of individual

servers. The number of neurotransmitters in the queue in such a case can be calculated by Little’s law which states

$$N = \frac{\lambda_Q R_S}{(1 - p_f)} \tag{22}$$

where  $N$  is the number of neurotransmitters in the queue,  $\lambda_Q$  is the arrival rate in the queue,  $R_S$  is the mean response time of the synaptic system and  $p_f$  is the probability of failure of axonal communication. It must be noted here that the number of neurotransmitters in the synapse would be more than the number of neurotransmitters in the queue. This is because neurotransmitters stay in the queue until they are served, they degrade or the presynaptic neuron re-uptakes them.

## 6. Simulation results

A wide variety of neurons occurs naturally, with their own respective response types. Evolution over millions of years has fine-tuned these various types of neurons to perform their specific tasks. However, for all this variability, the general characteristics of most neurons are similar. Various characteristics of neurons such as propagation speed through axons, effects of myelination, failure rates of axonal communication and synaptic distances are known from several studies [19,30–34]. Some of the key results for axons of average adult humans (age > 20 years) are compiled in Table 1.

Authors of [35] identify the  $Na^+$  ion absolute refractory period in human motor neurons to be nearly  $2.65 \pm 0.65$  ms. It should, however, be noted that this refractory period might vary with stimulus strength [36], but since it is a small change, it can be neglected when the analysis of an entire system is being considered. Additionally, the time required for vesicle release is identified in real-time by the authors of [13] to be nearly 1.3 ms. We would be using the mean value of 2.65 ms for  $Na^+$  ion absolute refractory period and 1.3 ms as the vesicle release latency in our analysis henceforth.

According to [24], the synaptic cleft between a presynaptic and a postsynaptic neuron is approximately 20 nm in humans. Furthermore, the probability of failure  $p_f$  of AP generation is taken at 3% according to the results of [17]. By (11), the time for diffusion of neurotransmitters with at least 97% confidence interval for a synaptic cleft width of 20 nm is derived to be nearly 0.7 ms.

Using these known parameters and assuming some of unknowns, we simulate a variety of scenarios in the next sections in MATLAB environment.

### 6.1. Case study of a nervous circuit: the knee-jerk reflex arc

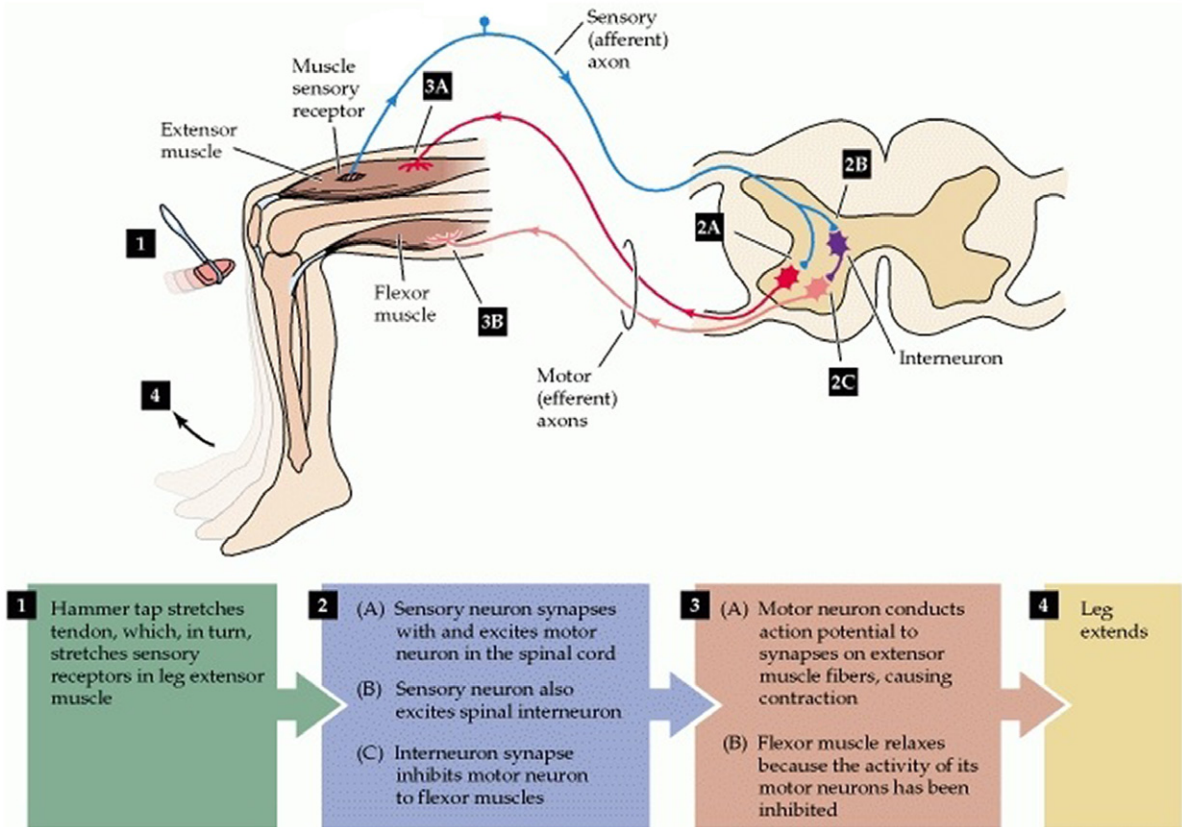
#### 6.1.1. Overview

One of the key advantages of using a queueing theory is the ease with which it can look at complex networks to find the average delays faced by packets. Under this motivation, we study a simple reflex action of the human body, known as the knee-jerk reflex, which is often used by physicians to test nervous diseases of the lower spinal cord. The knee-jerk reflex is an example of a monosynaptic nervous circuit



**Table 1**  
Axon parameters for standard adult (age > 20 years) [30–34].

Type	Myelin	Diameter (μm)	Propagation speed (m/s)
Tibial motor neurons	Yes	13–20	41–53
Femoral motor neurons	Yes	13–20	35–5
Sural sensory neurons	Yes	13–20	40–58
Preganglionic neurons	Yes	1–5	3–15
Postganglionic neurons	No	0.2–1.5	0.5–2.0



**Fig. 5.** The knee-jerk reflex arc [37].

in the body. This reflex is a reflex of proprioception which helps maintain posture and balance, allowing to keep one's balance with little effort or conscious thought. The process of eliciting a knee-jerk reflex is detailed in Fig. 5.

Striking the ligament of the knee with a reflex hammer just below the patella stretches the muscle spindle in the quadriceps muscle. Muscle spindles are sensory receptors present inside a muscle which detect changes in the length of the muscle. These spindles then produce a signal which travels back to the spinal cord via a sensory neuron and synapses in the L4 spinal segment.

The sensory neuron synapses with two motor neurons. A femoral motor neuron then conducts the impulse back to the quadriceps femoris muscle, triggering its contraction. Through an interneuron, a tibial motor neuron carries the signal to the hamstring muscle to relax it. This contraction, coordinated with the relaxation of the hamstring muscle causes the leg to kick [37].

### 6.1.2. Experimental results

Since the knee-jerk response is a very simple and efficient way to detect nervous diseases, it has been the center of various scientific studies for more than a hundred years. Many studies are present where the latencies from the time of stimulation to the time of response have been conducted. In [38], the knee-jerk reflex latencies are found and further divided as reflex latency, which is the time taken by the nervous components of the reflex arc, and the reflex motor time which is the time required by the muscles to move after receiving signals from motor neuron. The results of the study for a set of normal people are presented in Table 2.

### 6.1.3. Queueing model of knee-jerk circuit

Based on our discussion of the knee-jerk reflex, we present the queueing model for the circuit in Fig. 6. Application of an external impulse to the knee produces

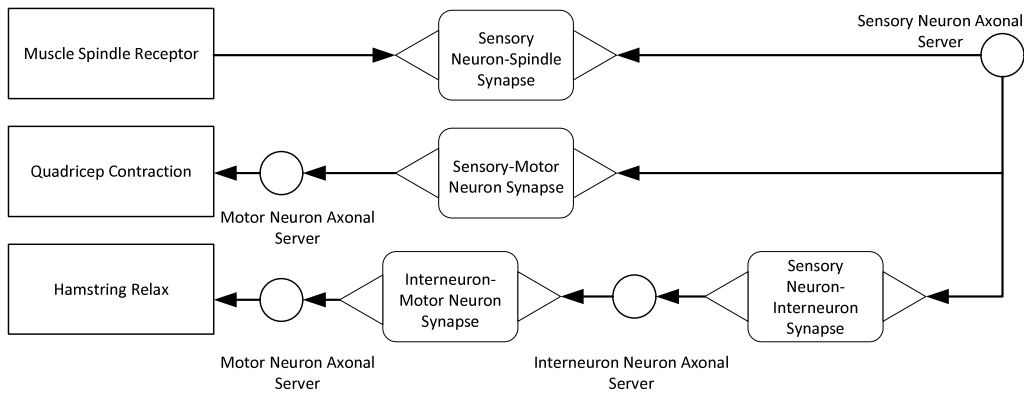


Fig. 6. Queuing model for knee-jerk reflex.

Table 2  
Knee-jerk reflex parameters [38].

Parameter	Value	Standard deviation
Number of test subjects	10	–
Mean age	23.3 years	3.1 years
Total reflex time	77.7 ms	16 ms
Reflex latency	23.4 ms	1.3 ms
Reflex motor time	54.2 ms	16.3 ms

sensations in the muscle spindle. The muscle spindles synapse with a sensory neuron making the first fork-join synaptic queue. This queue feeds the resultant summed EPSP signals to the Sensory neuron server. The sensory neuron is further connected with two fork-join queues, one for the motor neuron of qudricep and the other with an inhibitor interneuron. We can consider two independent fork-join queues for each of the nervous connections because the amount of neurotransmitter released is much higher than number of gates for either of the connections. The interneuron is further connected with the hamstring muscle though another fork-join queue. Each of these neurons has an axonal server as well.

6.1.4. Simulation of knee-jerk circuit

We now move on to simulate our knee-jerk reflex arc model. The average axonal lengths of the sensory and motor neurons for the knee-jerk reflex have not been estimated in any study, therefore, we have to approximate these. Since the axons of the sensory and the motor neurons run the length of the thigh to the base of the spinal cord near the hip, a good approximation would be to use the average distance between the hip and knee joint. According to US Center for Disease Control (CDC) statistics [39], the average upper leg length for males and females aged 20–29 is approximately 40 cm. Using (21), we simulate for the entire reflex arc over the conduction speeds for the range of values provided in Table 1 and show the results in Fig. 7.

The shaded region of the graph represents the range of values for reflex latency as described by Table 2. We see that a significant number of result data points fall within this range. This shows that application of the current model to the knee-jerk reflex nervous circuit gives similar results to those found by experimental studies. The results can be

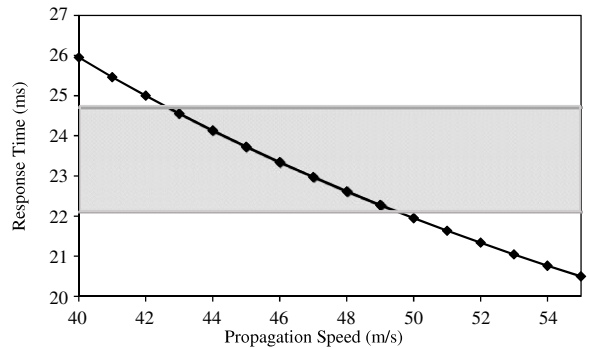


Fig. 7. Simulation of knee-jerk reflex over a range of propagation speeds.

further improved if axonal lengths and the latencies are measured from the same population or studies such as [35] are conducted on more subjects.

6.2. Effect of axon diameter

The diameter of an axon is directly proportional to its propagation speed. Taking the case of unmyelinated neuron, we varied the diameter of the axon to generate results shown in Fig. 8. The value for capacitance per unit area,  $c$ , is taken as  $1 \mu\text{F}/\text{cm}^2$ , the value for resistance per unit area  $r^*$  is taken as  $2000 \Omega/\text{cm}^2$  and the resistivity is taken as  $100 \Omega\text{m}$  according to [22]. We see that as the diameter is increased, the propagation speed increases which, in turn, causes the response time to decrease. The response time characteristics are similar to those observed in physical experiments [19,22].

6.3. Voltage decay along myelinated and unmyelinated neurons

The Human nervous system contains both myelinated and unmyelinated neurons [14]. Myelinated neurons are typically found in sensory and motor neurons while non-myelinated neurons are found in the brain and spinal cord.

Voltage decay along the axonal length is plotted in Fig. 9 using (2). We assume that the AP was at a maximum potential of 70 mV at the start of two neurons, one myelinated and one unmyelinated. For a myelinated neuron, the value

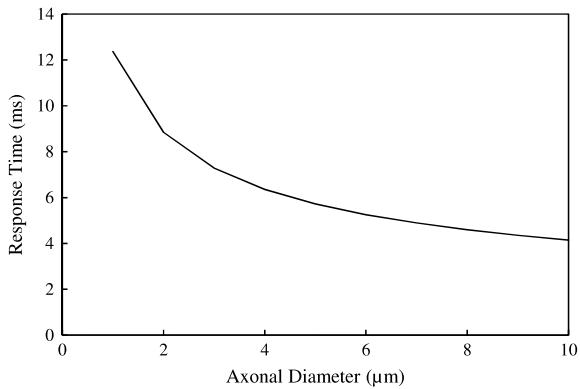


Fig. 8. Effect of axon diameter on response time.

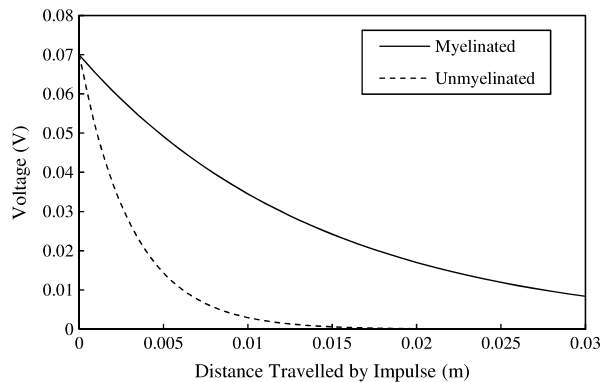


Fig. 9. Voltage decay along a neuron; myelinated vs. unmyelinated neurons.

of membrane resistance  $r_m$  is about 10–2000 times that of an unmyelinated neuron [22] depending on the thickness of the sheath of myelin outside the axon. For our current result, we use a value of 20 times. The resulting figure shows that over a similar length, the signal of an unmyelinated neuron decays more quickly. This was expected because as  $r_m$  increases, the length constant  $\lambda$  increases and the signal can travel longer distances. An interesting fact here is that as the membrane resistance increases for myelinated neurons, the membrane capacitance  $c_m$  decreases. This keeps the value of the time constant  $\tau$  given by  $\tau = c_m r_m$  nearly unchanged. The result agrees with experimental results that larger animals, needing slower AP decay, usually have myelinated neurons which operate at higher propagation speeds [19]. Similarly, sensory and motor neurons have myelination because they have to carry impulses over longer distances as compared to impulses carried over much smaller distances carried by the unmyelinated neurons in the human brain.

#### 6.4. Effect of frequency

The frequency of the input to a neuron is directly proportional to the internal resistance  $r_i$  and results in a decrease in the length constant. The results of Fig. 10 are generated using the PDF provided by (11) for a unit diffusion distance. Our results agree with the results of [7, 17] which state that as the frequency of the input signal to a neuron increases, the response time increases as well.

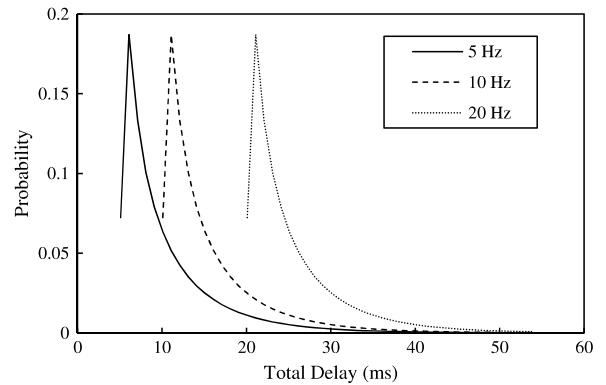


Fig. 10. Effect of frequency on response time distribution.

## 7. Conclusion

In this paper, we characterized neuro-spike communication between a presynaptic and a postsynaptic neuron by providing a queueing theory based model of the neuron. The model was evaluated on the basis of its mean response time characteristics. We found that the response time of neurons depends on a host of features including their environment, type of neuron, their physical dimensions and the input signals they are being provided by their respective stimuli. We also motivated the use of our technique and applied it to knee-jerk reflex arc. Our results agree with experimental finding regarding the characteristics of neurons. The model is very flexible and can be applied to neurons from other animals as well.

The current model can be used to gauge the response time characteristics of bio-inspired networks for new nanomachines and it may also help build new benchmarks for the study of the nervous system. Our future works aim to develop queueing based network models for more complex neural circuits such as those involved in human memory to understand the network behavior of sensing.

## Acknowledgments

This work was supported in part by the European Research Council (ERC) under grant ERC-2013-CoG #616922, by the Turkish Scientific and Technical Research Council under grant #109E257, by the Turkish National Academy of Sciences Distinguished Young Scientist Award Program (TUBA-GEBIP), and by IBM through IBM Faculty Award.

## References

- [1] M. Sauer, Reversible molecular photoswitches: A key technology for nanoscience and fluorescence imaging, *Proc. Natl. Acad. Sci. USA* 102 (27) (2005) 9433–9434.
- [2] S. Davis, Biomedical applications of nanotechnology implications for drug targeting and gene therapy, *Trends Biotechnol.* 15 (6) (1997) 217–224.
- [3] K.K. Jain, Nanotechnology in clinical laboratory diagnostics, *Clin. Chim. Acta* 358 (1) (2005) 37–54.
- [4] I.F. Akyildiz, F. Brunetti, C. Bazquez, Nanonetworks: A new communication paradigm, *Comput. Netw.* 52 (12) (2008) 2260–2279.
- [5] D. Malak, O.B. Akan, Molecular communication nanonetworks inside human body, *Nano Commun. Netw.* 3 (1) (2012) 19–35.

- [6] D. Malak, O.B. Akan, Communication theoretical understanding of intra-body nervous nanonetworks, *IEEE Commun. Mag.* 52 (4) (2014) 129–135.
- [7] E. Balevi, O.B. Akan, A physical channel model for nanoscale neuro-spike communications, *IEEE Trans. Commun.* 61 (3) (2013) 1178–1187.
- [8] D. Malak, M. Kocaoglu, O.B. Akan, Communication theoretic analysis of the synaptic channel for cortical neurons, *Nano Commun. Netw.* 4 (3) (2013) 131–141.
- [9] D. Malak, O.B. Akan, A communication theoretical analysis of synaptic multiple-access channel in hippocampal-cortical neurons, *IEEE Trans. Commun.* 61 (6) (2013) 2457–2467.
- [10] A. Sharp, A. Pannier, B. Wysocki, T. Wysocki, A novel telecommunications-based approach to hiv modeling and simulation, *Nano Commun. Netw.* 3 (2) (2012) 129–137.
- [11] B.J. Wysocki, T.M. Martin, T.A. Wysocki, A.K. Pannier, Modeling nonviral gene delivery as a macro-to-nano communication system, *Nano Commun. Netw.* 4 (1) (2013) 14–22.
- [12] T.M. Martin, B.J. Wysocki, J.P. Beyersdorf, T.A. Wysocki, A.K. Pannier, Integrating mitosis, toxicity, and transgene expression in a telecommunications packet-switched network model of lipoplex-mediated gene delivery, *Biotechnol. Bioeng.* 111 (8) (2014) 1659–1671.
- [13] D. Bruns, R. Jahn, Real-time measurement of transmitter release from single synaptic vesicles, *Nature* 377 (6544) (1995) 62–65.
- [14] E. Goldstein, *Sensation and Perception*, Cengage Learning, 2013.
- [15] A.L. Hodgkin, A.F. Huxley, A quantitative description of membrane current and its application to conduction and excitation in nerve, *J. Physiol.* 117 (4) (1952) 500.
- [16] R. Scott, A. Ruiz, C. Henneberger, D.M. Kullmann, D.A. Rusakov, Analog modulation of mossy fiber transmission is uncoupled from changes in presynaptic  $Ca^{2+}$ , *J. Neurosci.* 28 (31) (2008) 7765–7773.
- [17] M. Raastad, G.M. Shepherd, Single-axon action potentials in the rat hippocampal cortex, *J. Physiol.* 548 (3) (2003) 745–752.
- [18] D. Atdeley, *The Physiology of Excitable Cells*, Soc. Integ. Comp. Biol., 1971.
- [19] D. Debanne, E. Campanac, A. Bialowas, E. Carlier, G. Alcaraz, Axon physiology, *Physiol. Rev.* 91 (2) (2011) 555–602.
- [20] I. Tasaki, On the conduction velocity of nonmyelinated nerve fibers, *J. Integr. Neurosci.* 3 (02) (2004) 115–124.
- [21] W. Rall, R. Burke, W. Holmes, J. Jack, S. Redman, I. Segev, Matching dendritic neuron models to experimental data, *Physiol. Rev.* 72 (4) (1992).
- [22] J.G. Nicholls, A.R. Martin, B.G. Wallace, P.A. Fuchs, *From Neuron to Brain*, Vol. 271, Sinauer Associates, Sunderland, MA, 2001.
- [23] A. Manwani, C. Koch, Synaptic transmission: An information-theoretic perspective, in: *Advances in Neural Information Processing Systems*, 1998, pp. 201–207.
- [24] E.R. Kandel, J.H. Schwartz, T.M. Jessell, et al., *Principles of Neural Science*, Vol. 4, McGraw-Hill, New York, 2000.
- [25] L. Yavich, M.M. Forsberg, M. Karayiorgou, J.A. Gogos, P.T. Männistö, Site-specific role of catechol-o-methyltransferase in dopamine overflow within prefrontal cortex and dorsal striatum, *J. Neurosci.* 27 (38) (2007) 10196–10209.
- [26] W.R. Softky, C. Koch, The highly irregular firing of cortical cells is inconsistent with temporal integration of random EPSPs, *J. Neurosci.* 13 (1) (1993) 334–350.
- [27] A. Roxin, N. Brunel, D. Hansel, G. Mongillo, C. van Vreeswijk, On the distribution of firing rates in networks of cortical neurons, *J. Neurosci.* 31 (45) (2011) 16217–16226.
- [28] A.S. Lebrecht, W.J. Knottenbelt, Response time approximations in fork-join queues, in: *23rd UK Performance Engineering Workshop*, UKPEW.
- [29] A. Thomasian, A.N. Tantawi, Approximate solutions for  $m/g/1$  fork/join synchronization, in: *Proceedings of the 26th Conference on Winter Simulation*, Society for Computer Simulation International, pp. 361–368.
- [30] D.S. Stetson, J.W. Albers, B.A. Silverstein, R.A. Wolfe, Effects of age, sex, and anthropometric factors on nerve conduction measures, *Muscle Nerve* 15 (10) (1992) 1095–1104.
- [31] D.R.J. Laming, *The Measurement of Sensation*, Oxford University Press, 1997.
- [32] J.W. Albers, *Nerve Conduction Model*, University of Michigan Hospital, 1995. URL: <https://wiki.umms.med.umich.edu/download/attachments/133926019/SECTION4.pdf?version=1&modificationDate=1367434836000>.
- [33] D. Dumitru, M.J. Zwartz, Special nerve conduction techniques, in: *Electrodiagnostic Medicine*, second ed., Hanley and Belfus, Philadelphia, 2002, pp. 225–256.
- [34] I.S. Choi, Conduction studies of the saphenous nerve in normal subjects and patients with femoral neuropathy, *Yonsei Med. J.* 22 (1) (1981) 49–52.
- [35] J. Kimura, T. Yamada, R. Rodnitzky, Refractory period of human motor nerve fibres, *J. Neurol. Neurosurg. Psychiatry* 41 (9) (1978) 784–790.
- [36] J. Borg, Refractory period of single motor nerve fibres in man, *J. Neurol. Neurosurg. Psychiatry* 47 (4) (1984) 344–348.
- [37] D. Purves, G. Augustine, D. Fitzpatrick, *Neuroscience*, second ed., Sinauer Associates, 2001. URL: <http://www.ncbi.nlm.nih.gov/books/NBK11154/>.
- [38] T. Ryushi, T. Fukunaga, K. Yuasa, H. Nakajima, The influence of motor unit composition and stature on fractionated patellar reflex times in untrained men, *Eur. J. Appl. Physiol. Occup. Physiol.* 60 (1) (1990) 44–48.
- [39] C.D. Fryar, Q. Gu, C.L. Ogden, Anthropometric reference data for children and adults: United states, 2007–2010, in: *Vital and Health Statistics. Series 11, Data from the National Health Survey*. Vol. 252, 2012, pp. 1–48.



**Naveed A. Abbasi** received his B.Sc. degree in Electrical and Electronics Engineering from Air University, Islamabad, Pakistan, in 2007. He did his Masters from Northwestern Polytechnical University, Xi'an, PR China, with specialization in Signal and Information Processing in 2010. He is currently a research assistant in the Next-generation and Wireless Communication Laboratory and pursuing his Ph.D. degree at the Department of Electrical and Electronics Engineering, Koc University. His current research interests include molecular and nanoscale communications.



**Ozgur B. Akan** [M00-SM07] received his Ph.D. degree in electrical and computer engineering from the Broadband and Wireless Networking Laboratory, School of Electrical and Computer Engineering, Georgia Institute of Technology in 2004. He is currently a full professor with the Department of Electrical and Electronics Engineering, Koc University and the director of the Next-generation and Wireless Communications Laboratory. His current research interests are in wireless communications, nano-scale and molecular communications, and information theory. He is an Associate Editor of the *IEEE Transactions on Communications*, the *IEEE Transactions on Vehicular Technology*, the *International Journal of Communication Systems* (Wiley), the *Nano Communication Networks Journal* (Elsevier), and the *European Transactions on Technology*.